Enhancement of electrochemical biosensor performances using redox cycling at 3D sub-micrometer scale electrode architectures

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Introduction

Electrochemcial biosensors, Redox cycling, Carbon-MES



Approaches and Fabrication

Sensor configurations, Morphology



Enhancement of bio-sensing performance

Signal amplification, Sensitivity, Selectivity



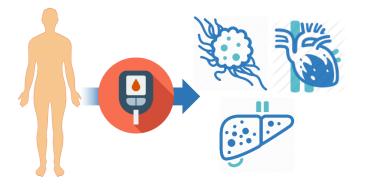
Summary & Future works

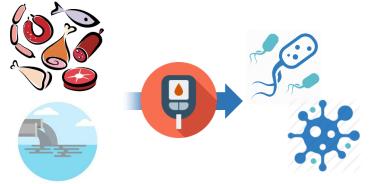


Electrochemical Biosensors: Applications

Health & safety

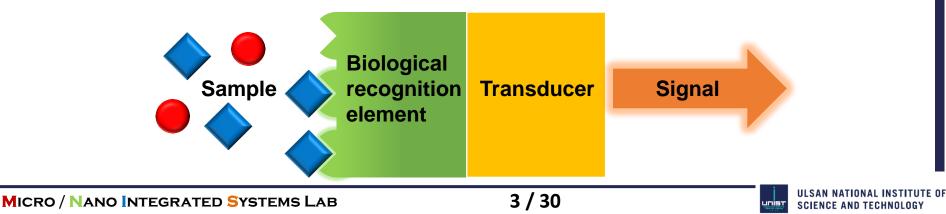
- Clinical diagnosis, food control, environmental screening





Biosensor classification

- Transducer types
 - Electrochemical, Optical, Electrical, Piezoelectric, Calorimetric



Electrochemical vs. Optical sensors

	Optical Sensor	Electrochemical Sensor
Sensitivity	Excellent	High
Selectivity	High	Good
Sample	Clear sample only	No limitation
Device configuration	Complex	Simple
Hand-held & Disposable	Difficult	Feasible
Cost	Relatively expensive	Cheap



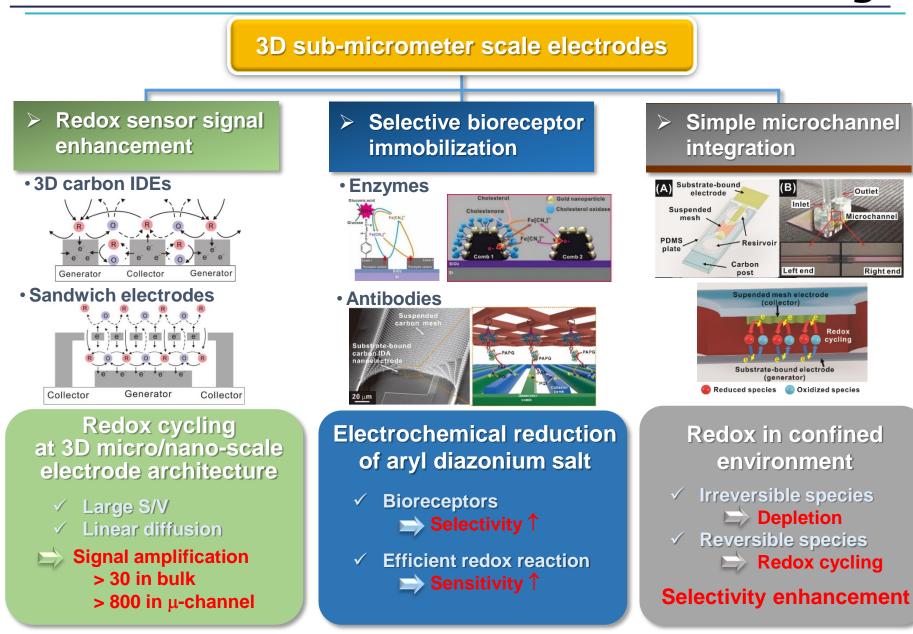


AmperometryVoltammetry

Coulometry
 EIS



Enhancement of electrochemical sensing



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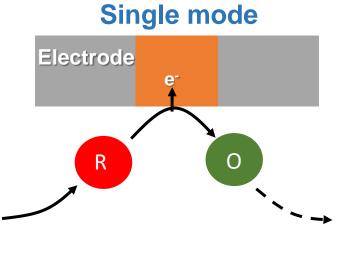
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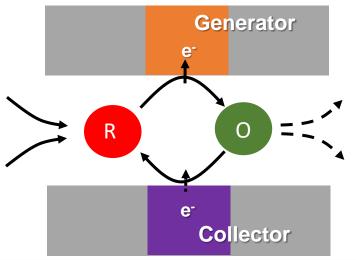
Redox cycling

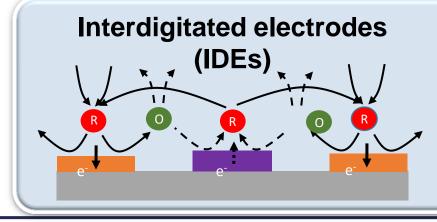
Sensitivity enhancement

- Amplifying Faradaic current signal

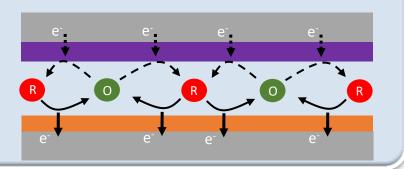


Dual mode (Redox cycling)





Sandwich electrodes



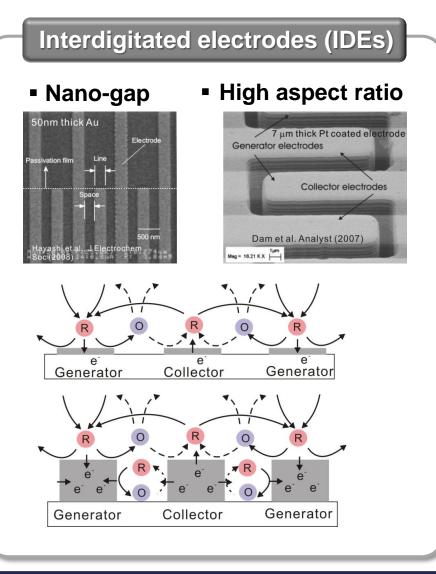
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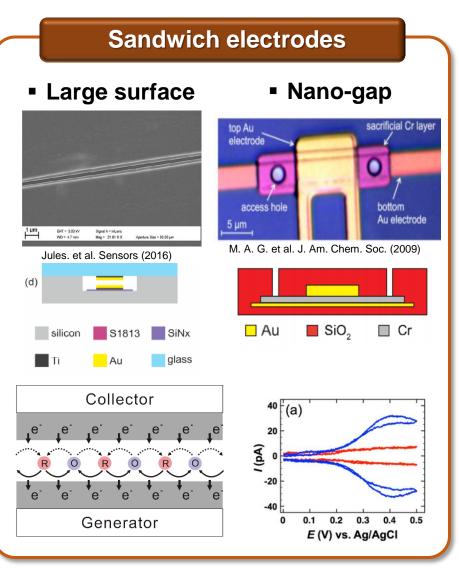
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Improvement of Redox cycling effect

Diffusion enhancement via electrode reconfiguration





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Improvement of Redox cycling effect

Limitations of previous approaches

Interdigitated electrodes (IDEs)

✓ Nano-gap:

- Expensive nanofabrication
- ✓ High aspect ratio:
 - **Complex MEMS process**
- Limitation in electrode gap reduction with high aspect ratio

Sandwich electrodes

Large electrode surface:
 Hassle alignment process

✓ Nano-gap:

- Sacrificial layer removal
- Difficulty in chip integration
- Small current signal

Carbon-MEMS-based nanoelectrodes

- ✓ Simple two-step nanoelectrode fabrication
- ✓ 3D architecture with complex design
- ✓ Electrode gap control via pyrolysis
- ✓ Comparable or even better current amplification

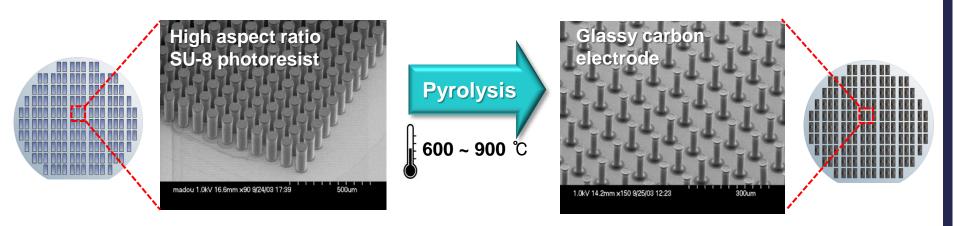


Carbon-MEMS

Polymer patterning + Pyrolysis

- Wafer-level simple fabrication of micro/nano carbon 3D structures
 - Conversion from polymer to glassy carbon
 - Conversion from insulator to conductor
 - Overcome limited manufacturability (brittleness)
 - Controllable geometry: photolithography, nano-imprint,

e-beam lithography, electrospinning.

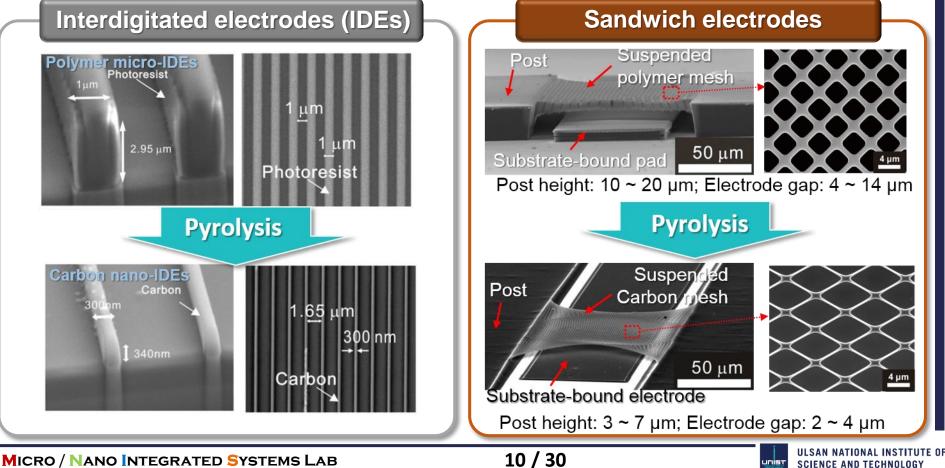




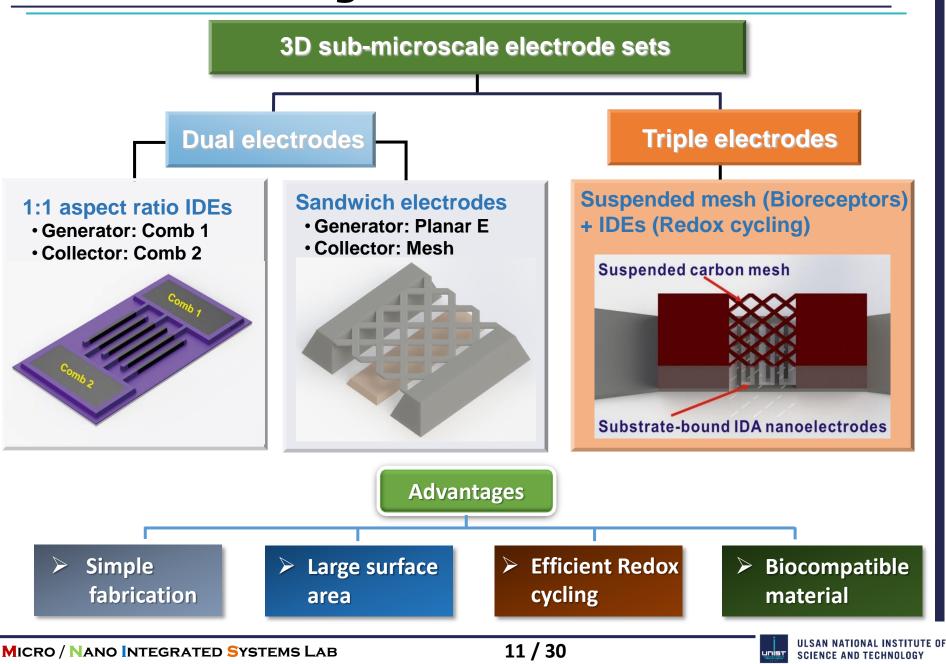
Carbon-MEMS

Polymer patterning + Pyrolysis

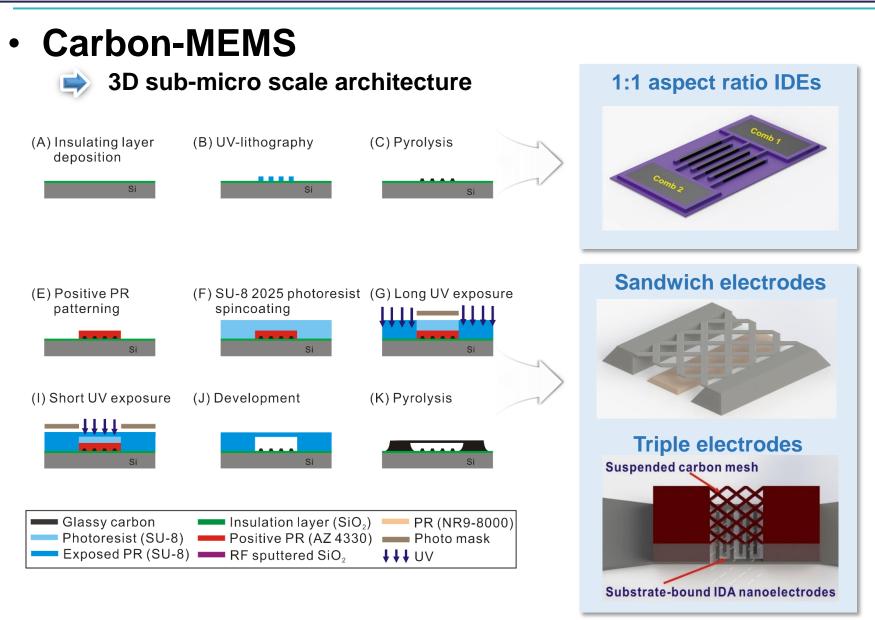
- Dramatic volume reduction up to 90%
 - Conversion from microstrucutres to nanostructures
 - Simple and easy fabrication of 1D carbon nanostructures



Electrode configurations



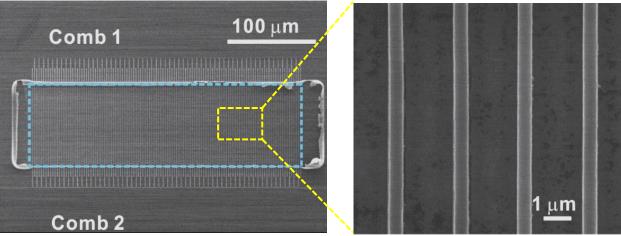
Fabrication



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Electrode morphology

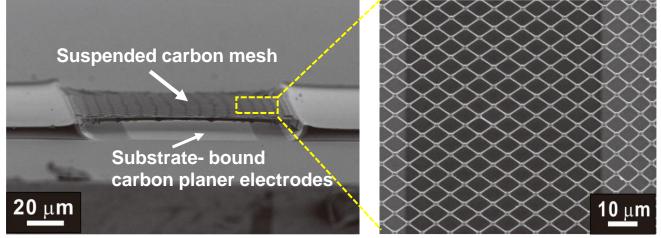
- Carbon-MEMS is Dual electrodes
 - Interdigitated Array (top view)



Dimensions:

- •Length: 100 µm
- Width: 620 nm
- Thickness: 650 nm
- Electrode gap ~ 1.9 µm

Sandwich electrodes (side & top view)



Dimensions

- Post height: ~ 4 µm
- Mesh thickness ~ 1 μm
- Mesh width ~ 300 nm
- Pad thickness ~ 600 nm
- Electrode gap ~ 2.4 μm





Electrode morphology

Carbon-MEMS
 Triple electrodes

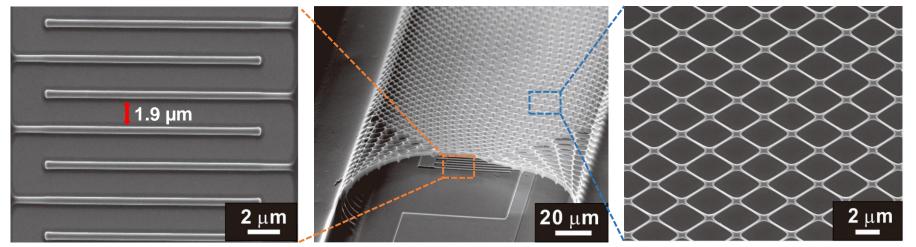
Substrate- bound carbon IDEs

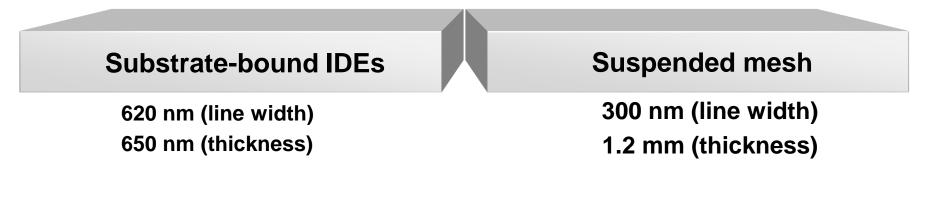
Suspended carbon mesh

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Signal amplification via redox cycling

Signal amplification

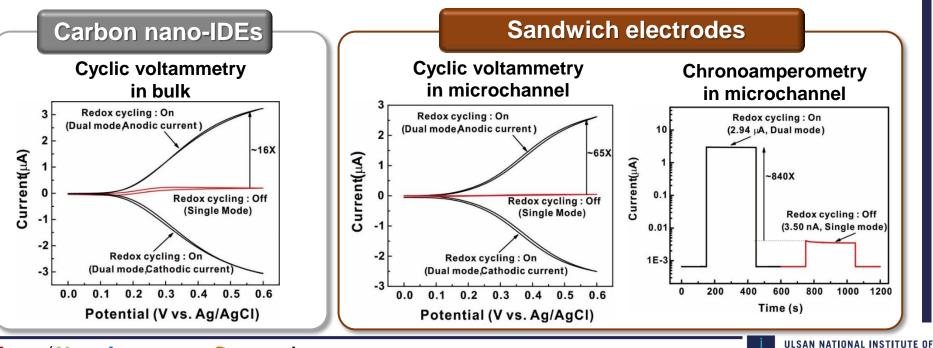
- Amplification factor = $\frac{I_{\text{Dual mode}}$ (Current signal with Redox cycling)

I Single mode (Current signal without Redox cycling)

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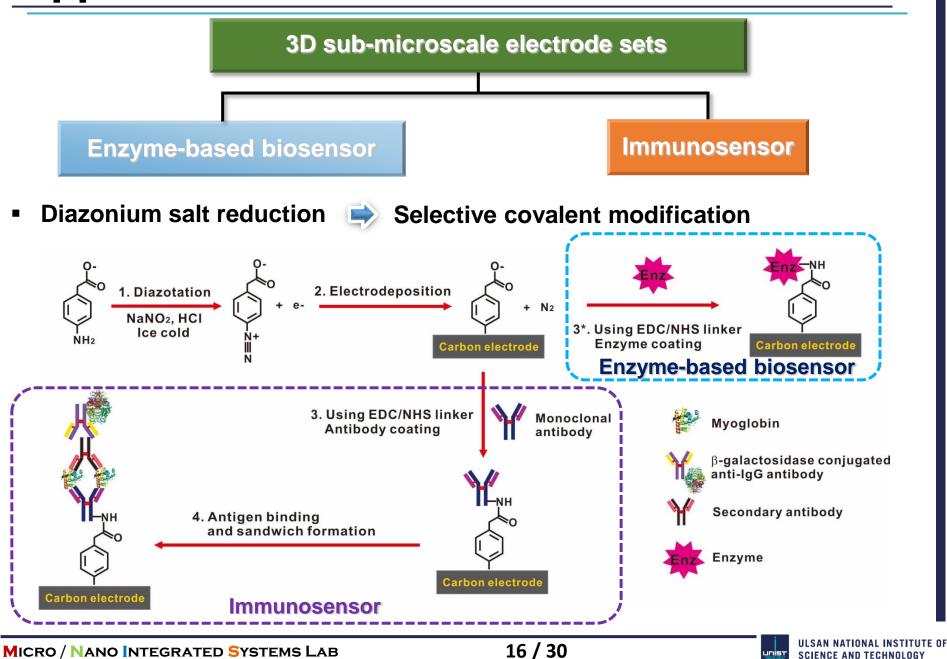
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- Linear diffusion between generator and collector
- Bulk vs Microchannel
 - Volume confinement effect in microchannel
 - Cyclic voltammetry (CV) vs Chronoamperometry



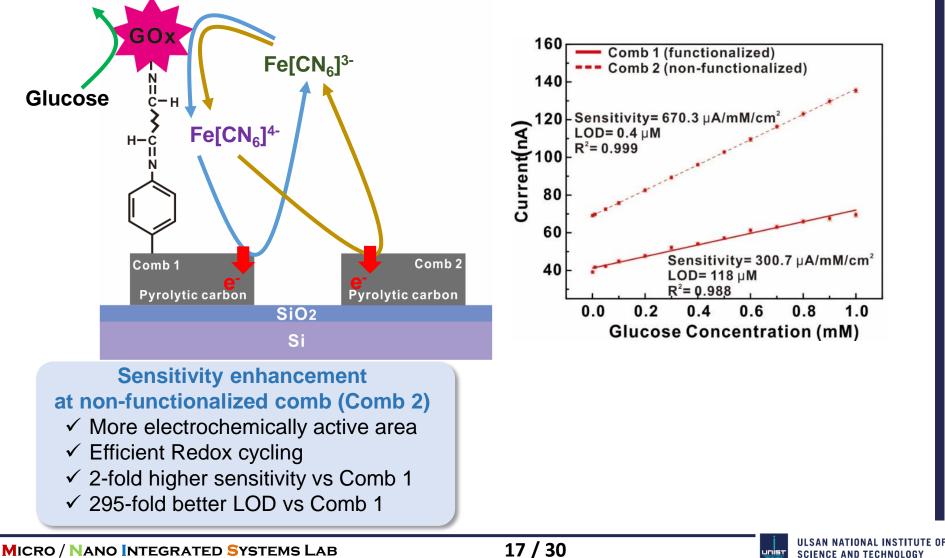
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Approaches for selective modification

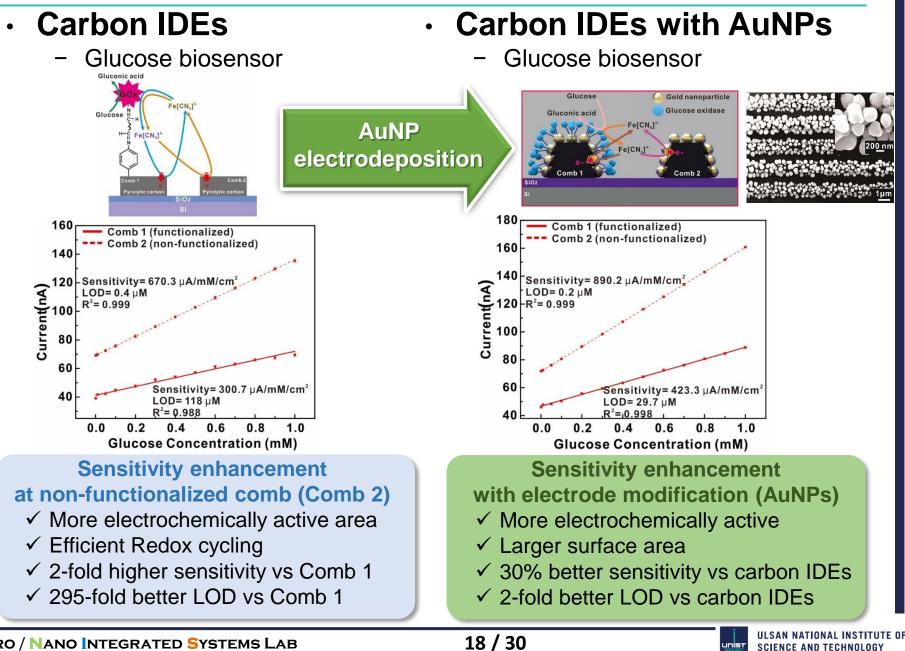


Enzyme-based biosensors

- Carbon IDEs
 - Glucose biosensor
- Gluconic acid



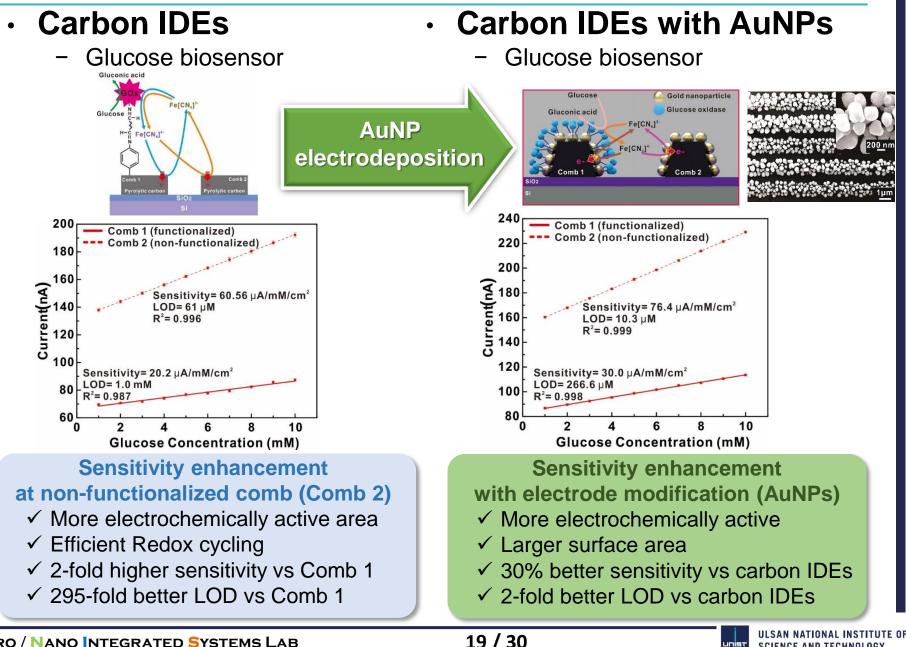
Enzyme-based biosensors



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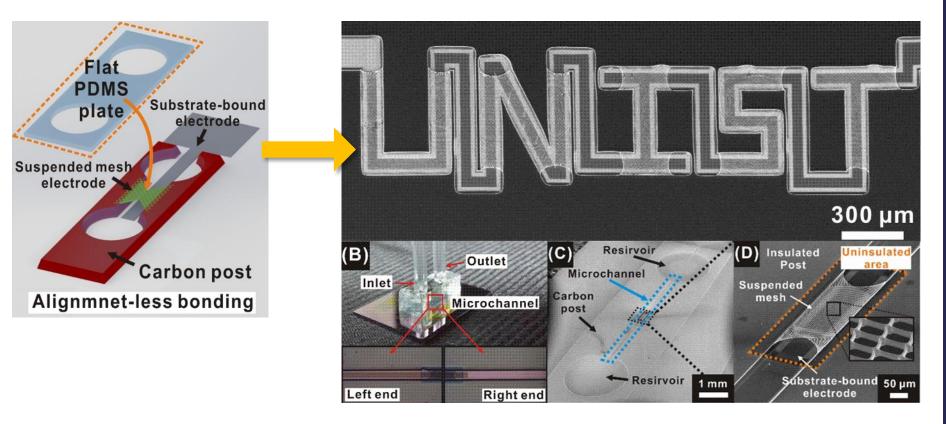
Enzyme-based biosensors



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Microchannel-integrated sandwich electrodes

- Alignment-less process
 - Flat PDMS plate + Sandwich electrodes
 - Carbon posts work as channels walls

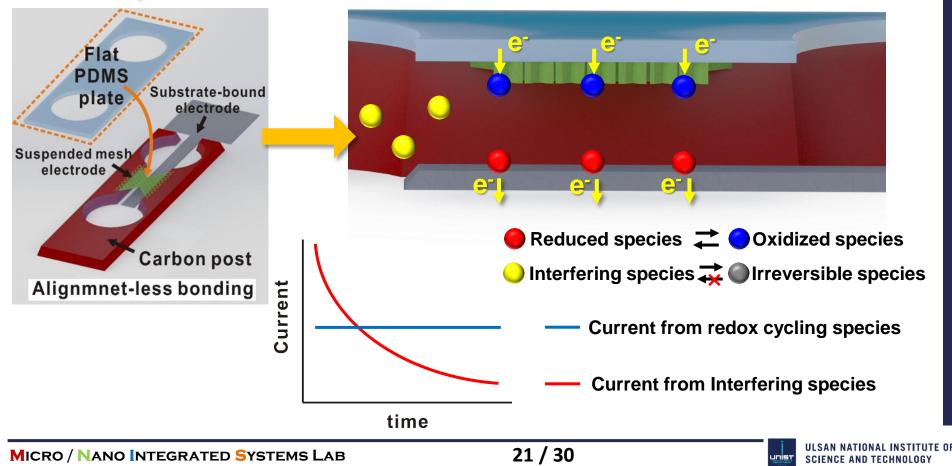




Confined volume in microchannel

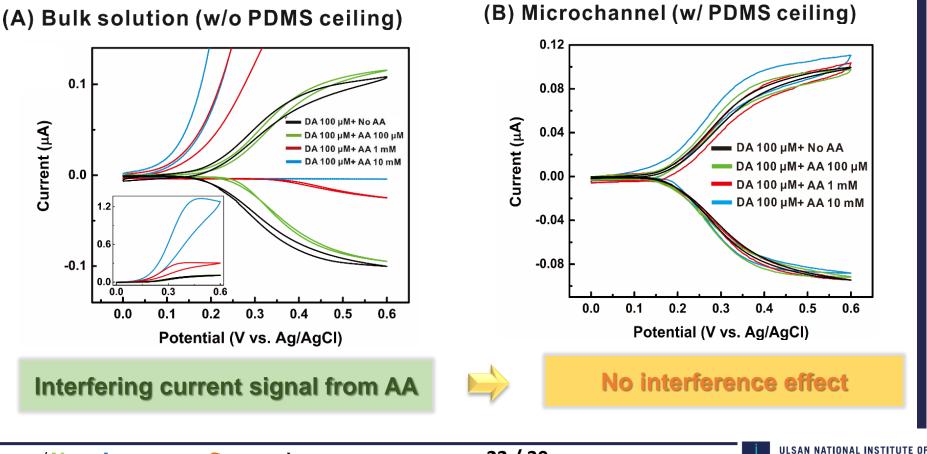
- Electrochemically reversible species Redox cycling
- Electrochemically irreversible species
 Depletion





Selective detection of dopamine

- Electrochemically reversible species: Dopamine (DA)
- Electrochemically irreversible species: Ascorbic acid (AA)



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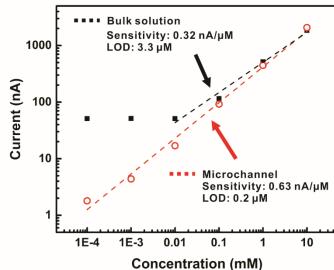
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Selective detection of dopamine

- Electrochemically reversible species: Dopamine (DA)
- Electrochemically irreversible species: Ascorbic acid (AA)

• Dopamine sensing (Bulk vs Microchannel)

- -LOD enhancement in microchannel
 - : 3.3 μ M (Bulk) \rightarrow 0.2 μ M (17 fold)
- Sensitivity enhancement in microchannel
 - : 0.32 nÅ/ μ M (Bulk) \rightarrow 0.63 nA/ μ M (2 fold)



Dopamine sensing in a microchannel

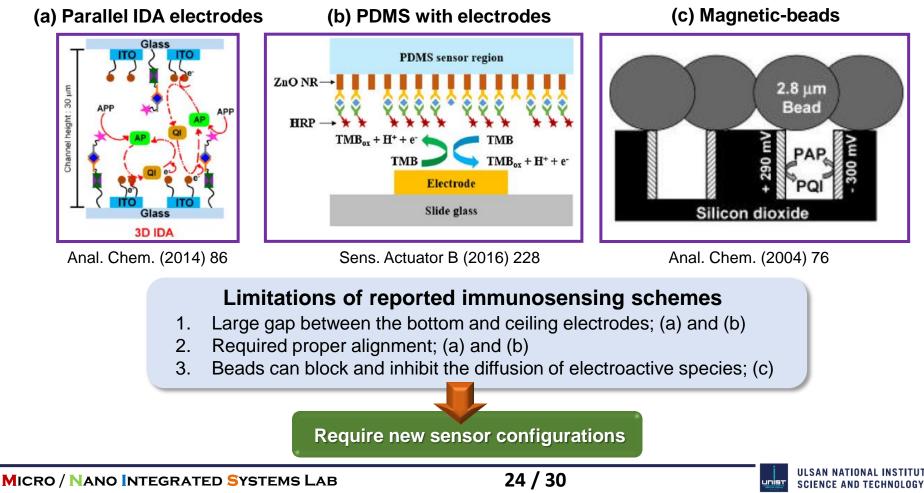
- ✓ Dopamine: 100 nM 10 mM
- ✓ Ascorbic acid: 1 mM
- ✓ PBS: 0.1 M



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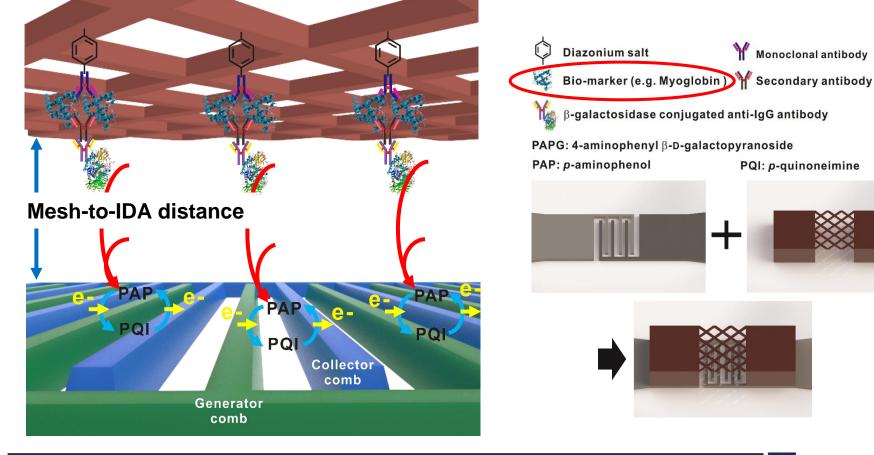
Electrochemical immunosensors

- Sandwich immunoassay
- Redox cycling
- Generation of redox substrate near the adjacent electrode



Suspended mesh + Substrate-bound IDEs

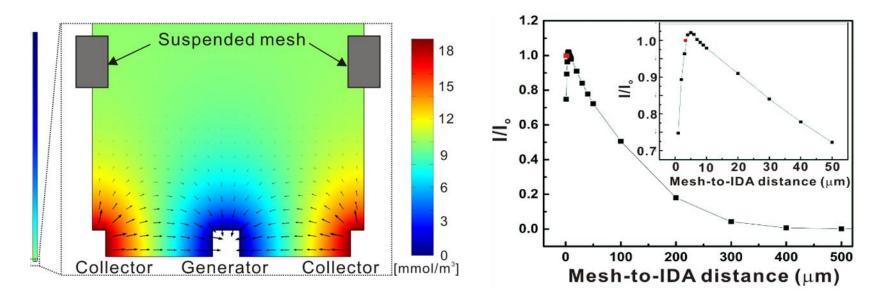
- Selective sandwich formation at suspended mesh
 - Generation of redox substrate (PAP) near carbon IDEs
 - Efficient Redox cycling (PAP \leftrightarrow PQI) at IDEs





Suspended mesh + Substrate-bound IDEs

- Effect of mesh-to-IDE distance
 - Simulation on diffusion-limited current signal

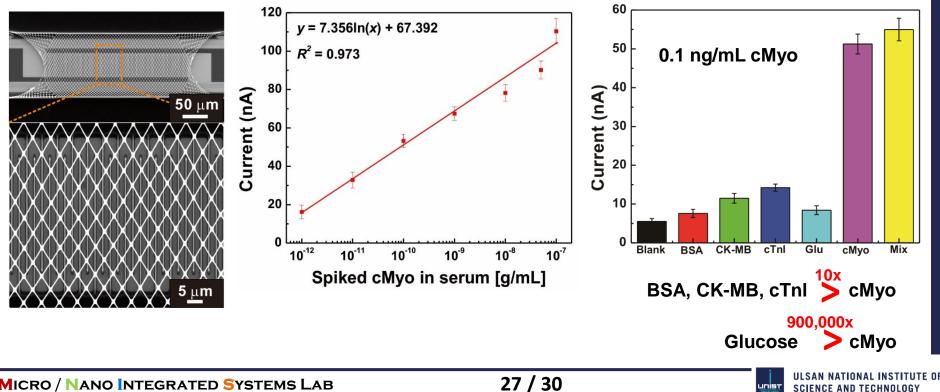


- $\checkmark\,$ Mesh-to-IDEs distance > 5 $\mu m \rightarrow$ small distance enhances diffusion of PAP
- ✓ Maximum current at 5 µm
- $\checkmark\,$ Mesh-to-IDEs distance < 5 $\mu m \rightarrow$ disturb diffusion among IDEs



Suspended mesh + Substrate-bound IDEs

- Mesh-to-IDEs distance ~ 3.3 μ m
 - Efficient production of redox species near IDEs
- Cardiac biomarker (Myoglobin) in human serum:
 - LOD ~ 0.48 pg/mL
 - High selectivity against interfering species



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Summary & Future works

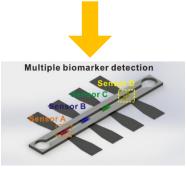
Summary

- Wafer-level batch fabrication via C-MEMS
 - 3D sub-micrometer scale electrode architectures
 - Simple and cost-effective processes
- Electrochemical sensor performance enhancement
 - Sensitivity
 - Selective bioreceptor immobilization near sensing area
 Efficient Redox cycling at 3D electrodes
 - Electrode surface modification with AuNPs
 - Selectivity
 - Bioreceptors (Enzymes, Antibodies)
 - Depletion effect in microchannel

Future works

- Multiple biomarker detection in a single chip
 - Microchannel integration
 - Integration of multiplex sensor array
 - Cholesterol, Glucose, CK-MB, Myoglobin, Troponin, etc.





3D triple carbon electrode set

Acknowledgements



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 - Prof. March Madou (UC Irvine)

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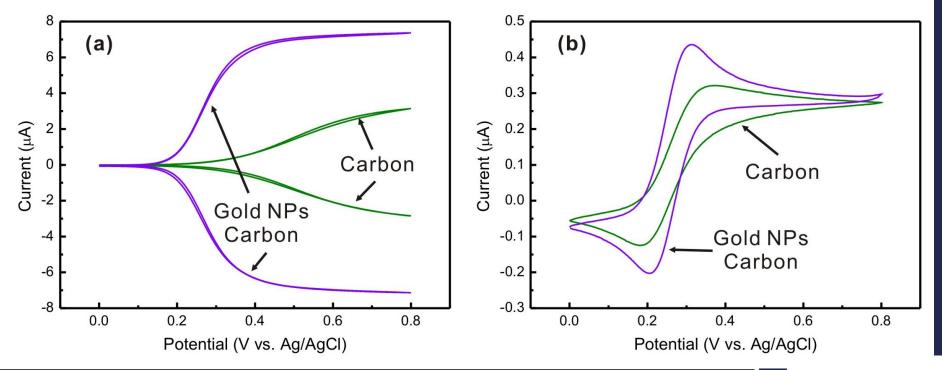
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Thank you for your attention



AuNPs/Carbon IDEs

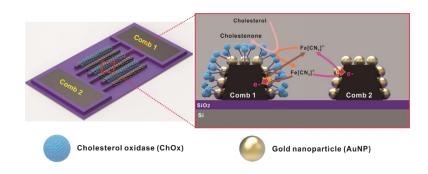
- Electrochemical characterization
 - Cyclic voltammetry
 - 10 mM [Fe(CN)₆]²⁺ in 0.1 M KCI
 - Carbon nanoelectrode
 - Width = 650 nm; Thickness = 650 nm
 - Current signal enhancement in dual mode

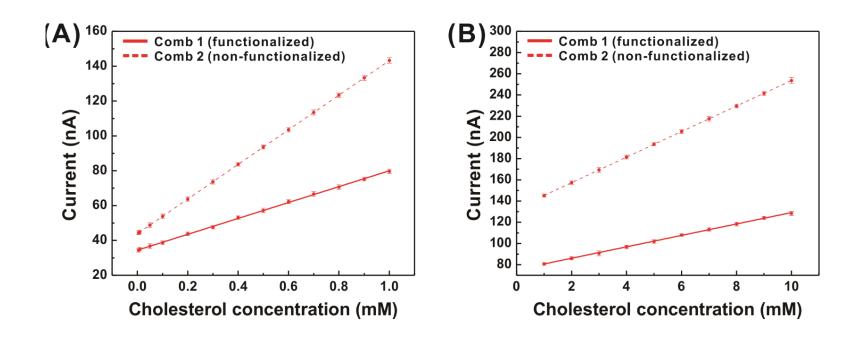




AuNPs/carbon IDEs

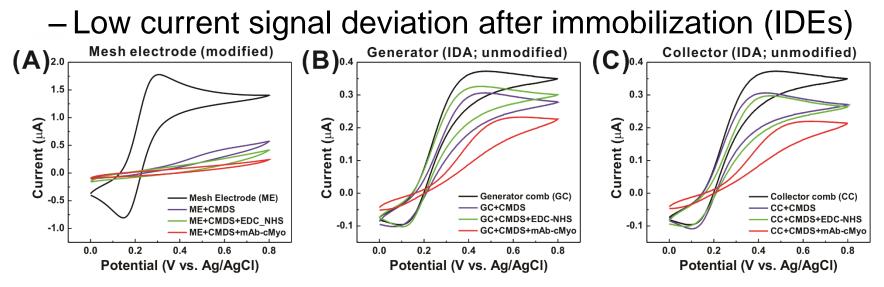
- Cholesterol sensors
 - Sensing range: 0.005-10 mM
 - Sensitivity ~994 μ A mM⁻¹ cm⁻²
 - LOD ~1.28 μM



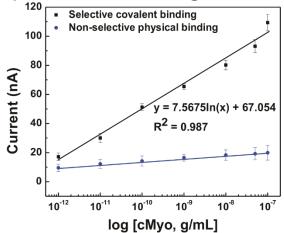




Effect of selective immobilization

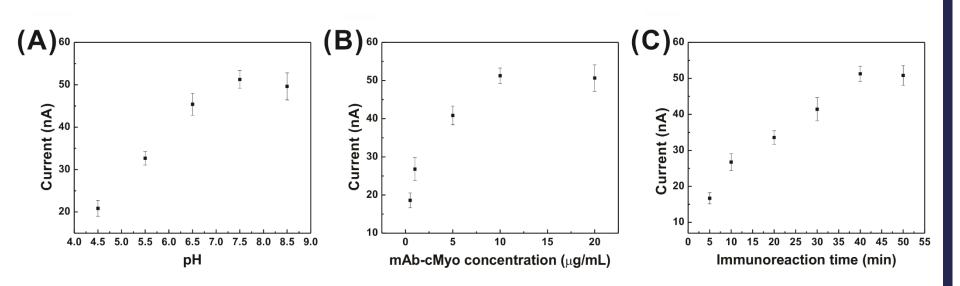


- Spontaneous physical binding reduces signal significantly.





 Effects of various sensor preparation conditions on the detection of 0.1ng/mL cMyo

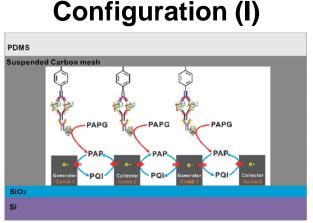




Immunosensing performance

Carbon 3D triple electrode

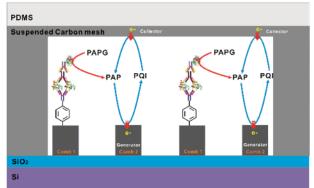
- 3D triple electrode set + selective immobilization
 - Reversible redox cycling (PAP \leftrightarrow PQI)
 - Generation of redox substrate (PAP) near the IDA electrode
- Characterization according to antibody binding site



Antibody binding site : suspended mesh generator & collector : IDA nanoelectrodes

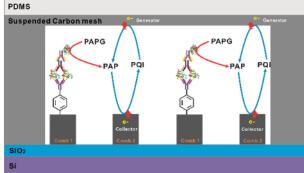
Configuration (II)

Configuration (III)



Antibody binding site : one comb of IDA Generator : the other comb of IDA Collector

: suspended mesh



Antibody binding site : one comb of IDA Generator

- : suspended mesh Collector
- : the other comb of IDA

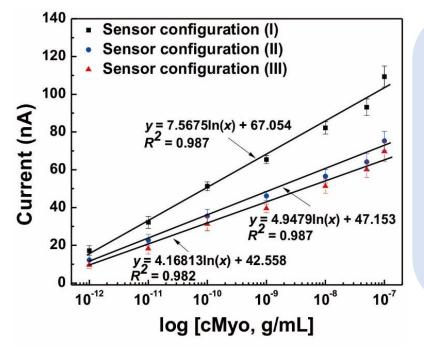
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Immunosensing performance

Carbon 3D triple electrode

- 3D triple electrode set + selective immobilization
 - Reversible redox cycling (PAP \leftrightarrow PQI)
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- Characterization according to antibody binding site



Sensitivity enhanced at sensor configuration (I)

- ✓ Small inter-electrode gap between IDEs
- ✓ Efficient redox cycling
- Large surface area of mesh enabling substantial biomolecule binding
- Efficient mass transfer

(I) Antibody site: suspended mesh, generator and collector: IDA nanoelectrodes;

(II) Antibody site: one comb of IDA nanoelectrodes, generator: the other comb of IDA nanoelectrodes, collector: suspended mesh;
 (III) Antibody site: one comb of IDA nanoelectrodes, generator: suspended mesh, collector: the other comb of IDA nanoelectrodes)

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